Mechanism and Control of Anthropomorphic Biped Robots

Hun-ok Lim\textsuperscript{1,2} & Atsuo Takanishi\textsuperscript{2,3}
\textsuperscript{1}Department of Mechanical Engineering, Kanagawa University
\textsuperscript{2}Humanoid Robotics Institute, Waseda University
\textsuperscript{3}Department of Mechanical Engineering, Waseda University

1. Introduction

Human beings, animals and some birds use their legs to move with great mobility, but we do not yet have a full understanding of their motion mechanism. The reason is that we lack man-made robots that use legs to obtain high mobility. We, especially, need two-legged robots that are able to adapt to human living environments such as offices and homes.

In order to analyze a human walking mechanism, some research groups studied about hydraulically-actuated or pneumatically-activated two-legged mechanisms in the 1960s. In 1973, a world’s first full-scale anthropomorphic robot, WABOT-1 (WAseda roBOT-1), was constructed at Waseda University as shown in Figure 1. It was able to communicate with a human in Japanese and to measure the distance and direction of objects using external receptors such as an artificial mouth, ears and eyes (Kato \textit{et al.}, 1973). Hydraulically powered, it used disproportionately large feet for stability. Also, it was able to grip and carry objects using the hands that were equipped with tactile sensors.

In 1983, WL-10R (Wasada Leg-10 Refined) was constructed using rotary type servo-actuators and carbon-fiber reinforced plastic. It was able to walk forwards and backwards, and turn on a flat plane. Based on the WL-10R, WHL-11 was developed by Wasada and Hitachi (Takanishi \textit{et al.}, 1985). It walked more than 85 km at Tsukuba Science Expo’85. In 1986-1995, WL-12 series robots that have a trunk and a 2-DOF waist was constructed to simulate human walking motion including his upper body motion as shown in Figure 2 (Takanishi \textit{et al.}, 1988; Li \textit{et al.}, 1992; Yamaguchi \textit{et al.}, 1995). They performed dynamic walking going up and down a stair with a height of 0.1 m and a slope of 10 deg (Takanishi \textit{et al.}, 1990). Also, they did not fall down and walked under an unknown external force of 100 N applied to their backs (Takanishi \textit{et al.}, 1991). However, the relative motion between their upper body and legs was difficult to be simulated.

An electrically powered human-sized biped humanoid robot, WABIAN (WAseda BIped humANoid), was constructed in 1996 for simulating human motion. It consists of a total of 35 DOF; two 3-DOF legs, two 10-DOF arms, two 2-DOF eyes, a 2-DOF neck and a torso with a 3-DOF waist (Setiawan \textit{et al.}, 1999). After 1996, WABIAN series robots were developed, and achieved quasi-human follow walking, emotional motion, dancing motion and so on (Setiawan \textit{et al.}, 1999; Lim \textit{et al.}, 2004a).
Section 2 deals with the mechanism and software of WABIAN-RII (WAsele BIped humANoid-Reffned II). The WABIAN-RII is a full-scaled biped humanoid robot that has 43 mechanical degrees of freedom (DOF). Section 3 addresses a locomotion pattern generation for biped humanoid robots. Its locomotion pattern is created online or offline according to the terrain conditions. Section 4 describes moment compensation control that is based on the motion of the waist and trunk. The motion of the waist and trunk is applied to maintain a good balance of the whole robot’s body while the path of the legs is controlled according to the terrain. Section 5 describes impedance control to reduce the contact/impact force of the landing foot. Impedance parameters are changed in real time depending on the gait phase. Section 6 addresses walking experiments to verify the effectiveness of the mechanism of the WABIAN serious robots, the moment compensation control and the impedance control. Section 7 describes conclusions. Also, future works are discussed to make more reliable control systems.

2. Mechanisms of WABIAN-RII

An adult-sized humanoid robot should be constructed to properly simulate human motion. We have been developing WABIAN-series robots since 1996. In this section, the mechanical and electrical structure of WABIAN-RII is proposed.

2.1 Mechanical Mechanisms

WABIAN-RII consists of two 6-DOF legs, two 7-DOF arms, two 3-DOF hands, two 2-DOF eyes, a 4-DOF neck and a torso with a 3-DOF waist (Lim et al., 2004a). Table 1 shows DOF of WABIAN-RII. Figure 3 shows a photo of WABIAN-RII. Its height is 1840 mm and its total weight is 127 kg. Table 2 and Table 3 show the weight and length distribution of each segment, respectively. The movable angle of the waist’s roll and yaw is ± 20 deg and ± 45 deg.
deg, respectively. The movable angle of the waist’s pitch is +30 deg and -10 deg. The movable angle of the knee is +90 deg and -0 deg. Figure 4 shows the movable angles of the pitch, roll and yaw, respectively. Duralumin, GIGAS (YKK Corp.) and CFRP (Carbon Fiber Reinforced Plastic) are mainly employed as its structural materials.

Fig. 2. Photo of WL-12RIII.

Fig. 3. Photo of WABIAN-RII.
2.2 Electrical systems
The trunk and legs of WABIAN-RII are driven by AC servo motors with reduction gears. The neck, hands and arms are actuated by DC servo motors with reduction gears. The eyes are driven by DC servo motors without reduction gears. Two CCD cameras that are attached to the head observe human environments. A force/torque sensor is attached to the wrist to detect interaction, and another force/torque sensor is attached between the ankle and the foot to measure ZMP. Also, a voice recognition system is installed.

WABIAN-RII is controlled by a PC/AT compatible computer PEAK-530 (Intel MMX Pentium 200 MHz CPU processor) run by MS-DOS 6.2/V (16-bit). TNT DOS-Extender SDK (Ver.6.1) is employed to extend the OS to a 32-bit. It has three counter boards, each with 24-bit 24 channels, three D/A converter boards, each with 12-bit 16 channels and an A/D converter board with differential 12-bit 16 channels to interface with sensors. The joint angles are sensed by incremental encoders attached to the joints, and the data are transferred to the computer through the counters. All the computations to control WABIAN-RII are carried out by the central computer, which runs the control program written in C language. The servo rate is 1 kHz. The computer system is mounted on the back of the waist and the servo driver modules are mounted on the upper part of the trunk. Electric power is the only external connection. Figure 5 shows the control system of WABIAN-RII.

<table>
<thead>
<tr>
<th>Parts</th>
<th>DOF</th>
</tr>
</thead>
<tbody>
<tr>
<td>Eye</td>
<td>2 (1 pitch, 1 yaw) × 2</td>
</tr>
<tr>
<td>Neck</td>
<td>4 (2 pitch, 1 roll, 1 yaw)</td>
</tr>
<tr>
<td>Waist</td>
<td>3 (1 pitch, 1 roll, 1 yaw) × 2</td>
</tr>
<tr>
<td>Hip</td>
<td>3 (1 pitch, 1 roll, 1 yaw) × 2</td>
</tr>
<tr>
<td>Knee</td>
<td>1 (1 pitch) × 2</td>
</tr>
<tr>
<td>Ankle</td>
<td>2 (1 pitch, 1 roll) × 2</td>
</tr>
<tr>
<td>Shoulder</td>
<td>3 (1 pitch, 1 roll, 1 yaw) × 2</td>
</tr>
<tr>
<td>Albow</td>
<td>1 (1 pitch)</td>
</tr>
<tr>
<td>Wrist</td>
<td>3 (1 pitch, 1 roll, 1 yaw) × 2</td>
</tr>
<tr>
<td>Hand</td>
<td>3 (thumb 1-DOF, index finger 1-DOF,</td>
</tr>
<tr>
<td></td>
<td>the other fingers 1-DOF) × 2</td>
</tr>
</tbody>
</table>

Table 1. DOF of WABIAN-RII.

<table>
<thead>
<tr>
<th>Parts</th>
<th>Weight (kg)</th>
<th>Parts</th>
<th>Weight (kg)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Foot</td>
<td>1.9 (×2)</td>
<td>Hand</td>
<td>0.5 (×2)</td>
</tr>
<tr>
<td>Ankle</td>
<td>7.8 (×2)</td>
<td>Wrist</td>
<td>0.5 (×2)</td>
</tr>
<tr>
<td>Knee</td>
<td>5.3 (×2)</td>
<td>Elbow</td>
<td>0.9 (×2)</td>
</tr>
<tr>
<td>Head</td>
<td>2.4</td>
<td>Shoulder</td>
<td>5.9 (×2)</td>
</tr>
<tr>
<td>Neck</td>
<td>6.4</td>
<td>Waist</td>
<td>20.6</td>
</tr>
<tr>
<td>Trunk</td>
<td>52.0</td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

Table 2. Segment weight of WABIAN-RII.
<table>
<thead>
<tr>
<th>Parts</th>
<th>Length (mm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Height</td>
<td>1840</td>
</tr>
<tr>
<td>Width</td>
<td>706</td>
</tr>
<tr>
<td>Depth</td>
<td>533</td>
</tr>
<tr>
<td>Between foot and ankle</td>
<td>142</td>
</tr>
<tr>
<td>Between ankle and knee</td>
<td>300</td>
</tr>
<tr>
<td>Between knee and hip</td>
<td>353</td>
</tr>
<tr>
<td>Between hip and waist</td>
<td>176</td>
</tr>
<tr>
<td>Between waist and neck</td>
<td>537</td>
</tr>
<tr>
<td>Between neck and head</td>
<td>332</td>
</tr>
<tr>
<td>Upper arm</td>
<td>263</td>
</tr>
<tr>
<td>Lower arm</td>
<td>247</td>
</tr>
</tbody>
</table>

Table 3. Segment length of WABIAN-RII.

Fig. 4. Movable range of WABIAN-RII.

(a) Pitch’s movable angle  
(b) Roll’s movable angle  
(c) Yaw’s movable angle
3. Locomotion Pattern Generation

A biped locomotion phase can be classified into a contact, a single and a double supporting phase to generate a leg motion. During the single supporting phase, one foot is not constrained to the ground but the other foot is on the ground. As soon as the heel of the swinging foot reaches the ground, the single supporting phase is changed to the contact phase. If the toe and heel of the swinging foot contacts on the ground, the phase becomes a double supporting phase. Fig. 6 shows a locomotion phase for a leg pattern generation.

The smooth motion of the foot according to terrain conditions, \( x_f \), can be generated by using a sixth degree polynomial considering the angle, the angular velocity, the angular acceleration and the height from the ground to the foot (Lim et al., 2004b). Three constraints of the foot position and orientation come from the selection of initial and final values:

\[
x_f(t_0) = x_0, \quad x_f(t_f) = x_f, \quad x_f(t_m) = x_m,
\]

where \( t_0, t_m \) and \( t_f \) are the initial, intermediate and final time of a step, respectively.

The position and orientation of the foot have an additional four constraints that are the zero initial and final velocity and acceleration:

\[
\dot{x}_f(t_0) = 0, \quad \ddot{x}_f(t_0) = 0, \quad \dot{x}_f(t_f) = 0, \quad \ddot{x}_f(t_f) = 0.
\]

The sixth order polynomial for a foot motion is written as follows:

\[
x_f(t) = a_0 + a_1 t + a_2 t^2 + a_3 t^3 + a_4 t^4 + a_5 t^5 + a_6 t^6,
\]

and the velocity and acceleration along the path are clearly

\[
\dot{x}_f(t) = a_1 + 2a_2 t + 3a_3 t^2 + 4a_4 t^3 + 5a_5 t^4 + 6a_6 t^5,
\]

\[
\ddot{x}_f(t) = 2a_2 + 6a_3 t + 12a_4 t^2 + 20a_5 t^3 + 30a_6 t^4.
\]
Combining Equation (3) and Equation (4) with the seven constraints, the seven coefficients \( (a_0 \cdots a_6) \) can be obtained. Then, substituting these coefficients for Equation (3), the foot motion pattern is obtained. In addition, a knee and waist pattern is created by inverse kinematics.

Fig. 6. Locomotion phase.

4. Moment Compensation Control

When a biped humanoid robot walks, moments generated by the motion of the legs make it unstable (Lim & Takanishi, 2005). To cancel the moments, a moment compensation control is discussed in this section.

4.1 Concept of Zero Moment Point

Consider a single supporting phase in which one foot is not constrained to the ground. As shown in Figure 7, the supporting polygon (stable region) is made by the contact points between the foot sole and the ground. To maintain the dynamic equilibrium of a biped humanoid robot, the ground reaction force should act at an appropriate point on the foot sole. It means that the ZMP (Zero Moment Point) exists at a point where the total forces and moments are equal to zero in the support polygon (Vukobratovic et al., 1970). In this study, the ZMP is arbitrarily set in the stable region.

Fig. 7. ZMP in supporting polygon.

4.2 Moment Compensation

A world coordinate frame \( \mathcal{F} \) is fixed on the ground, and a moving coordinate frame \( \tilde{\mathcal{F}} \) is attached to the center of the waist of a biped humanoid robot to define mathematical quantities. Considering that the humanoid robot is a set of particle model, the balancing moment around a contact point \( p \) in a supporting polygon can be expressed with respect to the world coordinate frame \( \mathcal{F} \) as
where \( r_p \) is the position vector of the point \( p \) from the origin of the frame \( \mathcal{F} \). \( m_i \) is the mass of the particle \( i \) of the biped humanoid robot, \( r_i \) and \( \ddot{r}_i \) denote the position and acceleration vectors of the particle \( i \) with respect to \( \mathcal{F} \), respectively. \( G \) is the gravitational acceleration vector. \( T \) is the moment vector acting on the contact point \( p \). \( r_j \) denotes the position vector of the particle \( j \) relative to the frame \( \mathcal{F} \), respectively. Let the ZMP be on the point \( p \). The moment \( T \) will be a zero vector by the ZMP concept. Therefore, equation (5) can be rewritten relative to the moving frame \( \mathcal{F}_m \) as follows:

\[
\sum_{i=1}^{n} m_i (\ddot{r}_i - \ddot{r}_{zmp}) \times (\ddot{r}_i + \ddot{r}_q + G + \dot{\omega} \times \ddot{r}_i + 2\dot{\omega} \times \ddot{r}_i + \ddot{\omega} \times (\dot{\omega} \times \ddot{r}_i)) \\
- \sum_{j=1}^{n} ((\ddot{r}_j - \ddot{r}_{zmp}) \times \ddot{F}_j + \ddot{M}_j) = 0,
\]

where \( \ddot{r}_{zmp} \) is the position vector of the ZMP with respect to \( \mathcal{F} \). \( r_q \) is the position vector of the origin of \( \mathcal{F} \). \( \dot{\omega} \) and \( \ddot{\omega} \) denote the angular velocity and acceleration vectors, respectively.

In case that the upper body is modeled as a four-mass model as shown in Figure 8, three moment components generated by the motion of the particles of the legs, \( M = [M_x, M_y, M_z]^T \), can be written as follows:

\[
m_s (\dddot{x}_s \dddot{x}_s - \dddot{x}_s \dddot{z}_s) + m_t (\dddot{x}_t - \dddot{z}_{zmp}) (\dddot{x}_t + \dddot{x}_q + g_x) \\
- m_t (\dddot{x}_t - \dddot{z}_{zmp}) (\dddot{x}_t + \dddot{x}_q + g_x) \\
+ m_w (\dddot{x}_w - \dddot{z}_{zmp}) (\dddot{x}_w + \dddot{x}_q + g_x) \\
- m_w (\dddot{x}_w - \dddot{z}_{zmp}) (\dddot{x}_w + \dddot{x}_q + g_x) = -M_y(t),
\]

\[
m_s (\dddot{y}_s \dddot{y}_s - \dddot{z}_s \dddot{y}_s) + m_t (\dddot{y}_t - \dddot{z}_{zmp}) (\dddot{y}_t + \dddot{y}_q + g_y) \\
- m_t (\dddot{y}_t - \dddot{z}_{zmp}) (\dddot{y}_t + \dddot{y}_q + g_y) \\
+ m_w (\dddot{y}_w - \dddot{z}_{zmp}) (\dddot{y}_w + \dddot{z}_q + g_y) \\
- m_w (\dddot{y}_w - \dddot{z}_{zmp}) (\dddot{y}_w + \dddot{z}_q + g_y) = -M_z(t),
\]

\[
m_s (\dddot{x}_s \dddot{y}_s - \dddot{y}_s \dddot{x}_s + 2(\dddot{x}_s \dddot{y}_s + \dddot{y}_s \dddot{y}_s) \dddot{w}_z + (\dddot{x}_s \dddot{y}_s + \dddot{y}_s \dddot{y}_s) \dddot{w}_z) \\
+ m_t (\dddot{x}_t - \dddot{z}_{zmp}) (\dddot{y}_t + \dddot{y}_q + g_y) \\
- m_t (\dddot{y}_t - \dddot{z}_{zmp}) (\dddot{x}_t + \dddot{x}_q + g_x) \\
+ m_w (\dddot{x}_w - \dddot{z}_{zmp}) (\dddot{y}_w + \dddot{y}_q + g_y) \\
- m_w (\dddot{y}_w - \dddot{z}_{zmp}) (\dddot{x}_w + \dddot{x}_q + g_x) = -M_x(t),
\]

where \( m_s \) denotes the mass of both shoulders including the mass of the arms. \( m_t \) is the mass of the torso including the head, shoulders and arms, and \( m_w \) is the mass of the waist. \( \ddot{r}_s = [\dddot{x}_s, \dddot{y}_s, \dddot{z}_s]^T \) and \( \ddot{r}_w = [\dddot{x}_w, \dddot{y}_w, \dddot{z}_w]^T \) are the position vectors of the neck and the waist with respect to the \( \mathcal{F} \), respectively. \( \ddot{r}_s = [\dddot{x}_s, \dddot{y}_s, \dddot{z}_s]^T \) is the position vector of the shoulder with respect to the neck frame.
These moment equations are interferential and non-linear because each equation has the same variables, $\ddot{z}_w$ and $\ddot{z}_t$. Thus, it is difficult to derive analytic solutions from equations (7), (8) and (9). We assume that neither the waist nor the trunk particles move vertically, and the trunk arm rotates on the horizontal plane only as

\begin{equation}
\ddot{z}_t = 0, \quad \ddot{z}_w = 0, \quad \ddot{z}_q = 0, \quad z_t - \bar{z}_{zmp} = \text{const.}, \quad z_w - \bar{z}_{zmp} = \text{const.}
\end{equation}

(10)

We put the terms about the motion of the particles of the upper body on the left-hand side as unknown variables, and the terms about the moments generated by the particles of the lower-limbs on the right-hand side as known parameters. The decoupled and linearized ZMP equations can be written as

\begin{align}
\dot{M}_y + \dot{M}_w &= \dot{M}_y(t), \\
\dot{M}_x + \dot{M}_w &= \dot{M}_x(t), \\
m_t\ddot{\theta}_t &= \dot{M}_z(t),
\end{align}

(11), (12), (13)

where

\begin{align}
\dot{M}_y &= m_t(\ddot{z}_t - \ddot{z}_{zmp})\ddot{x}_t - m_t g_s \ddot{x}_t, \\
\dot{M}_w &= m_w(\ddot{z}_w - \ddot{z}_{zmp})\ddot{x}_w - m_w g_s \ddot{x}_w, \\
\dot{M}_x &= -m_t(\ddot{z}_t - \ddot{z}_{zmp})\ddot{y}_t + m_t g_s \ddot{y}_t, \\
\dot{M}_w &= -m_w(\ddot{z}_w - \ddot{z}_{zmp})\ddot{y}_w + m_w g_s \ddot{y}_w, \\
\dot{M}_y(t) &= -M_y - (m_t(\ddot{z}_t - \ddot{z}_{zmp})\ddot{x}_q + m_t g_s \ddot{x}_{zmp} \\
&\quad + m_w(\ddot{z}_w - \ddot{z}_{zmp})\ddot{x}_q + m_w g_s \ddot{x}_{zmp}), \\
\dot{M}_x(t) &= -M_x - (-m_t(\ddot{z}_t - \ddot{z}_{zmp})\ddot{y}_q - m_t g_s \ddot{y}_{zmp}).
\end{align}

(14)
\[
M_s(t) = \dot{M}_s(t) - m_l(x_t - \bar{x}_{zmp})(\ddot{y}_t + \ddot{y}_q) - m_l(\ddot{y}_t - \ddot{y}_{zmp})(\dddot{x}_t + \dddot{x}_q) + m_w(x_w - \bar{x}_{zmp})(\dddot{y}_w + \dddot{y}_q) - m_w(\dddot{y}_w - \dddot{y}_{zmp})(\dddot{x}_w + \dddot{x}_q),
\]

where \(\theta_t\) is the vertical angle of the trunk. \(l\) is the length between the neck and the shoulder. \(\bar{M}_{st}\) and \(\dot{\bar{M}}_{st}\) denote the roll’s and the pitch’s trunk components of the moments, respectively. \(\bar{M}_{xw}\) and \(\dot{\bar{M}}_{xw}\) are the moment components of the waist’s roll and pitch, respectively. \(\bar{M}_{xw}, \dot{\bar{M}}_{xw}, \bar{M}_{st}\) and \(\dot{\bar{M}}_{st}\) become the known functions because they are calculated by the motion of the lower-limbs and the time trajectory of the ZMP. In steady walking, they are periodic functions because each particle of the biped humanoid robot and the ZMP move periodically with respect to the frame \(\bar{F}\). Comparing the Fourier transform coefficients of both sides of each equation, the approximate periodic solutions of the pitch’s and roll’s waist and trunk, \(\ddot{y}_w, \dddot{x}_w, \ddot{y}_t, \dddot{x}_t\) and \(\theta_t\) can be obtained.

### 4.3 Recursive Calculation

It is difficult to calculate the compensatory motion due to six unknown variables such as \(\ddot{y}_w, \dddot{x}_w, \ddot{y}_t, \dddot{x}_t, \theta_t\) and \(\theta_w\). Each equation is represented as a Fourier series. Using the Fourier transform coefficients, the approximate periodic solutions of the pitch’s and roll’s waist and trunk can be obtained. The approximate solutions are substituted into the moment equation (6), and the errors of moments generated by the waist and trunk motions are calculated according to the planned ZMP. These errors are accumulated to the right-hand side of equations (11), (12) and (13). The approximate solutions are computed again. These computations are repeated until the errors fall below a certain tolerance level. As a result, the strict periodic solutions of the nonlinear equations are obtained by a convergent regularity. The limit value of an accumulated moment error on each axis, \(E_n\), is estimated as follows:

\[
E_n = \frac{2E_{n-1} + e_{n-1}}{2},
\]

where \(e_n\) is the \(n\)th moment error.

Figure 9 shows the block diagram for the compensatory motion of the waist and trunk. We numerically verified the convergence of the solutions using computer simulations. A 30 deg turning walking was simulated with the step time of 1.28 s/step and the step width of 0.2 m/step. Among the ten, the biped humanoid robot turned at the fifth and sixth step. Figure 10 shows the convergence of the turning walking. In this simulation, the errors of the pitch’s, roll’s and yaw’s moments drop below 0.1 Nm after ten iterations.

Figure 11 shows the convergence of the trunk motion depending on the walking speed when the trunk length is 0.6[m]. In these simulations, the errors of the ZMP are dropped below 1.0[mm]. We can see that the recursive method does not take so much time in calculating the compensatory motion of the trunk and waist.

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Fig. 9. Calculation of compensatory motion.

Fig. 10. Moment errors in turning walking.
4.4 Trunk Motion for Complete Walking

This compensation control is also applicable to a complete walking. By regarding the complete walking motion as one periodic walking motion and applying the control method to it, the compensatory motion of the waist and trunk in steady and transitional walking can be derived. However, the biped humanoid robot must have a long period of standing time before starting and after stopping.

Assuming that the waist is immovable, the pitch’s and the roll’s moment components of equation (6) can be changed as

\[ (\ddot{z}_t - \ddot{z}_{zmp})\dddot{x}_t - g_z \dddot{x}_t = -A(t), \]  
\[ (\ddot{z}_t - \ddot{z}_{zmp})\dddot{y}_t + g_z \dddot{y}_t = B(t), \]  

where

\[ A(t) = \frac{M_y(t) + m_w(\ddot{z}_w - \ddot{z}_{zmp})\dddot{x}_w - m_w g_z \dddot{x}_w}{m_t}, \]
\[ B(t) = \frac{M_y(t) - m_w(\ddot{z}_w - \ddot{z}_{zmp})\dddot{y}_w - m_w g_z \dddot{y}_w}{m_t}. \]  

Consider only the motion of the trunk around the pitch’s axis to investigate the compensatory motion. The transfer function \( \tilde{y}_t(\omega) \) in the frequency domain can be expressed as

\[ \tilde{y}_t(\omega) = \frac{2p}{\omega^2 + p^2}q = \left(-\frac{1}{p - j\omega} + \frac{1}{p + j\omega}\right)q, \]

where

\[ p = \sqrt{\frac{g_z}{\ddot{z}_t - \ddot{z}_{zmp}}}, \quad q = -\frac{1}{2g_z}\sqrt{\frac{g_z}{\ddot{z}_t - \ddot{z}_{zmp}}}. \]
According to the ZMP concept, $\ddot{z}_{\text{ZMP}}$ in equation (20) is zero. Equation (19) is generally known as Lorentz function, and its primitive function is written as

$$\ddot{y}(t) = qe^{-\rho|t|}. \quad (21)$$

We can imagine from equation (21) that the casual law may not be applied anymore. If the walking speed of the biped humanoid robot is increased, it goes without saying that $\ddot{y}(t)$ affects stability more badly. The trunk, therefore, should be in motion earlier than the shift of the ZMP on the ground to cancel the moments produced.

The relationship between the motion of the trunk and the applied force was simulated. When the biped humanoid robot was not in motion, an impulse moment 1000 Nm was applied to the trunk’s pitch. Figure 12 shows the pitch’s motion of the trunk. In this simulation, we can see that the compensatory motion of the trunk should begin with a view of balancing before and after the impulse moment is applied to the biped humanoid robot.

![Fig. 12. Motion of trunk’s pitch](image)

**5. Impedance Control**

It is difficult for a biped humanoid robot to avoid instability caused by the impact/contact forces produced between the landing foot and the ground during dynamic walking. So, an impedance control is discussed in this section to guarantee higher stability with high speed walking (Lim et al., 2004c).

When a human walks, he controls his leg muscles for shock absorption and posture. His muscles are relaxed to absorb the impact/contact force just before his landing foot makes an initial contact, while his muscles are hardened to maintain the balance after landing (Kazerooni & Waibel, 1988; Park & Kim, 1999). We pay attention to the elasticity of the biped humanoid robot like a human.

Suppose that the biped foot is connected to the ground with a spring and a damper model. A force/torque sensor is mounted between the foot and the ankle to measure the impact/contact force as shown in Figure 13. Also, an ankle coordinate frame $F_a$ is fixed on the center of the ankle, and an end-effector coordinate frame $F_z$ is attached at the ZMP.
The impact/contact force between the landing foot and the ground, \( F \in \mathbb{R}^6 \), can be written as

\[
M_d \ddot{p} + D_d \dot{p}_e + K_d p_e = F, \\
p_e = p - p_d.
\]  

(22)

where \( M_d \in \mathbb{R}^{6 \times 6} \) is the desired mass matrix. \( D_d \in \mathbb{R}^{6 \times 6} \) and \( K_d \in \mathbb{R}^{6 \times 6} \) are the damping and stiffness matrices, respectively. \( p \in \mathbb{R}^6 \) and \( p_d \in \mathbb{R}^6 \) denote the actual and desired position vectors of the foot, respectively. The joint angles of the leg can be measured by the proper encoders attached to each joint. Then, \( p \) is calculated by forward kinematics. The reaction force \( F \) is measured by the force/torque sensor.

Fig. 13. Ankle and ZMP coordinate frames.

The angular velocity vector \( \dot{\theta} \) that is commanded to the landing leg can be obtained as follows:

\[
\dot{\theta} = J^{-1}(\theta) \dot{p}
\]

(23)

where

\[
\dot{p} = M_d^{-1} \int (F - D_d p_e - K_d p_e).
\]

(24)

For the absorption of the impact forces and the stable posture of the biped humanoid robot, an impedance control method is employed as shown in Figure 14. During the whole walking cycle, the position control based on the walking pattern is basically employed. The joint angles are measured by the encoders, and the actual position of the foot is calculated by using forward kinematics. The parameters in the impedance control are modulated depending on the gait phase as follows:

(1) in the swinging phase, only the position control is employed,(2) in the contact/double supporting phase, the impedance control with large viscosity is employed to reduce the impact/contact force, (3) in the first half of the single supporting phase, the impedance
control with large stiffness is applied to increase the momentum reduced, and (4) in the last half of the single supporting phase, the walking pattern changed by the impedance control is interpolated to the desired walking pattern.

Fig. 14. Impedance control systems.

6. Experiments

For a biped humanoid robot to walk stably on terrains, the moment compensation control and the impedance control were described in the above sections. In this section, the effectiveness of the control methods is tested through dynamic walking experiments.

6.1 Impedance Control Test

The position control and the impedance control are experimented using a WABIAN serious robot. In this experiment, the impedance control was applied to the ankle joint. Dynamic walking is realized with the step speed of 1.28 s/step and the step length of 0.15 m/step (Lim et al., 2004c).

The contact forces and moments of the left foot are shown in Figure 15 (a)-(b), respectively. The experimental results are plotted after 5.12 s. The pitch’s contact forces and moments are largely reduced in the last step. Figure 16 (a) and (b) illustrate the desired and actual x-and y-ZMP. The ZMP errors in the impedance control are small. So, we can say that the position-based impedance control is effective in suppressing the impact/contact forces and moments.

6.2 Compensation Control Test

The walking direction and length can be determined by a vision tracking and an auditory system (Lim et al., 2004b). The vision system is initialized, and both hands of a human are specified as tracking points during the walking. The auditory system recognizes the walking length that is defined by compiling the text file of grammar rules. Using the locomotion pattern generator based on the visual and the auditory information, a locomotion pattern with 25 steps (four steps forwards, five steps to the right, four steps backwards, six steps to the left and six steps on the spot) is created.
Fig. 15. Reaction forces and Moments on the left foot. IC denotes the impedance control.

(a) Pitch’s moment $M_y$
(b) Pitch’s reaction force $F_y$.

Fig. 16. ZMP trajectories under two different controls. IC: Impedance control.

(a) X-ZMP
(b) Y-ZMP
In the experiment, dynamic walking with 25 steps was achieved with the walking speed of 0.96 s/step using the moment compensation control. The response trajectories show a good accuracy of following the reference joint trajectories as shown in Figure 17. It means that the compensatory motion of the waist and trunk is used effectively.

(a) Pitch’s angle of knee joint.

(b) Pitch’s angle of hip joint.

Fig. 17. Angle response of the right leg.

7. Conclusion and Discussion

The mechanism of a 43 DOF biped humanoid robot WABIAN-RII was described to simulate human motions was described. For the humanoid robot to walk stably on various terrains, its functions should be separated. Its waist and trunk carries out the function of stability, while its legs work out the function of the locomotion. A locomotion pattern generation was discussed which used a polynomial. In the pattern generation, the direction of the walking and the length of the step can be determined by visual and auditory information. Also, a moment compensation control was presented to balance its body, which was based on the motion of the waist and trunk. In addition, an impedance control method was discussed to absorb the impact/contact forces generated between the landing foot and the ground, which can adjust the impedance parameters to make relaxed and hardened motions like a human. The experimental results show that the impedance and the moment compensation control are effective for the sock absorption and stability. However, for a more reliable locomotion, biped humanoid robots must be able to adjust the time of the locomotion. If the walking time is suddenly changed, unnecessary acceleration is able to occur, and the errors of the ZMP can be increased. To solve these problems, a new control method will be introduced which uses the motion of the upper-lims, and the impedance control should be considered in all the joints. Especially, the moment of the yaw should be compensated to deal with high speed walking.
7. References


This book covers many aspects of the exciting research in mobile robotics. It deals with different aspects of the control problem, especially also under uncertainty and faults. Mechanical design issues are discussed along with new sensor and actuator concepts. Games like soccer are a good example which comprise many of the aforementioned challenges in a single comprehensive and in the same time entertaining framework. Thus, the book comprises contributions dealing with aspects of the Robotcup competition. The reader will get a feel how the problems cover virtually all engineering disciplines ranging from theoretical research to very application specific work. In addition interesting problems for physics and mathematics arises out of such research. We hope this book will be an inspiring source of knowledge and ideas, stimulating further research in this exciting field. The promises and possible benefits of such efforts are manifold, they range from new transportation systems, intelligent cars to flexible assistants in factories and construction sites, over service robot which assist and support us in daily live, all the way to the possibility for efficient help for impaired and advances in prosthetics.

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